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(54) Title: ELECTRODE STRIPS FOR TESTING SMALL VOLUMES

(57) Abstract

A test strip comprising a support carries an active electrode and a counterelectrode, and a layer of material within which a small volume of liquid to be tested can be distributed and provide contact between the electrodes, and wherein an analyte-specific reagent is coated on the material. The layer of material can conveniently be provided in the form of a tape from which sections can be cut or used sequentially.

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Electrode Strips for Testing Small Volumes

Field of the Invention

This invention relates to electrode strips for testing small volumes of, say, whole blood.

5 Background of the Invention

Diabetes is one of the most common endocrine conditions. Sufferers must monitor their blood glucose level frequently. This is usually achieved by the use of small test strips which detect blood glucose.

Problems commonly experienced by users of these test strips are an inadequate amount of blood on the test strip and bad placement of the blood on the test strip. A number of devices have addressed this problem by using sample chambers that fill by capillary action. The sample is retained in close proximity to the electrodes which facilitate the measurement of the specific analyte in the sample; see EP-A-0170375 and US-A-5141868.

Such known devices comprise electrodes deposited on a non-conducting substrate, coated with a reagent system specific for the analyte of interest and housed within a cavity whose dimensions are sufficiently small to allow introduction of a sample, e.g. 2.5-3 µL in volume, by capillary action. The extent to which these devices can be miniaturized is limited by both the manufacturing tolerances and the signal-to-noise ratio achievable with their chemistry.

US-5820551 discloses a test strip comprising a support carrying a working electrode and a counter electrode, and an enzyme and a mediator that are coated on the active electrode. A drop of whole blood can provide a conducting path between the electrodes, and the concentration of glucose in the blood can be determined. The active electrode is exposed to a whole blood sample without an intervening membrane or other whole blood filter.

WO-A-98/55856 (published after the priority date claimed for this Application) discloses an analyte-specific reagent coated on the conductive layer, and a monofilament mesh laid over the reagent and the reference electrode. A sample application area is provided at one edge of the mesh.

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Summary of the Invention

According to a first aspect of the present invention, a test strip comprises a support carrying an active electrode and a counterelectrode, and a layer of a material within which a small volume of liquid to be tested can be distributed and provide contact between the electrodes, and wherein an analyte-specific reagent such as one component of a redox reaction, e.g. an enzyme, co-factor or mediator, is coated on the material. In particular, the invention provides a test strip for blood glucose, in which the sample requirement is very small, and efficient reaction kinetics are achieved by the application of the reagents in a novel manner.

The reagent-coated material may itself be in tape form. According to a second aspect of the invention, a flexible tape is of a material within which liquid can be distributed and on which are coated discrete areas of at least one component of a redox reaction.

15 Description of the Invention

In accordance with this invention, any one or more of the components of a redox reaction, e.g. an enzyme such as glucose oxidase or glucose dehydrogenase, a co-factor and a mediator may be applied to a mesh or membrane which is placed over the device. For the purpose of illustration only, the invention may be described with reference to an enzyme-coated mesh. Whichever component or components are used, when the sample is added, they are solubilised quickly and form an efficient reaction medium that can provide contact between the separate electrodes of the test strip. In this manner, the reaction will proceed rapidly and without diffusion barriers. This reaction configuration is particularly indicated in cases where the sample volume is low, the sample is viscous (such as with whole blood) and a rapid reaction is required.

In a typical embodiment of the invention, the sensor test strip consists of two electrodes, one of which acts as a working electrode and another which acts as a counter, reference electrode. The end of the working electrode that is exposed to the sample has a mediator in intimate contact with it. The test strip effectively provides a reaction chamber defined by these two electrodes

and an additional sheet, overlying the electrodes, which has been pre-coated with the redox enzyme and any necessary co-factor for that enzyme. The reaction chamber may also comprise further sheets of material and/or wetting agents, e.g. a surfactant, or cell-lysing materials (which may be placed in any one of the overlying sheets). In this manner, the active enzyme is not coated onto the conductor which forms the working electrode but is provided in a separate layer above it which, in turn, effectively forms the solution phase of the reaction chamber. When combined with lateral flow, conditions are created that approach efficient mixing in a stirred reaction chamber.

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In an example of the invention, a silver chloride/silver reference/counter electrode is located adjacent to a carbon electrode. Typically, for this purpose, a pair of printed carbon electrodes is printed on a non-conducting substrate, and then silver/silver chloride is printed on one of the carbon electrodes to function as the reference/counter electrode. A non-conducting ink is printed over the carbon electrodes and the substrate, in order to define a portion of each electrode as a contact pad for insertion into a meter and another portion on each electrode away from the contact pad as the sensing area where the sample is received.

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A mediator for the enzyme cofactor NADH is then prepared and deposited onto the electrode from aqueous solution by pipetting. A further layer containing NAD is then deposited onto the working electrode.

A monofilament mesh material is coated with a surfactant and then with a solution containing glucose dehydrogenase via pipetting, ink jet-coating or dip-coating, and is placed over the two electrodes to form a reaction chamber. This reaction chamber may be defined further by additional printing, or by the use of a top layer to form an edge fill cavity. For example, a second non-conducting ink printed on top of the mesh material, and then a cover tape is applied on top of the mesh in such a way as to leave an extended area of the mesh exposed for sample application.

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The device allows the application of a small volume of sample (typically 1 μ L or less) to the mesh extension. This is followed by flooding of the device

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sensing area with sample, bringing it into intimate contact with the measuring electrodes.

Devices having an edge fill are described in WO-A-98/55856. They can be simply adapted, in accordance with the present invention. In particular, reference may be made to Fig. 1 in WO-A-98/55856; components of this invention are the support (1), electrodes (2/3), mesh material (6) and tape (7); in addition, reagent is provided on the mesh material. Such a device can work by application at its edge, to a sample. This is particularly valuable in cases where it is difficult to extract the sample. Other configurations will be evident to one skilled in the art, including combinations of one or more of the cofactor, mediator or the enzyme coated onto the overlying mesh or membrane sheets. The choice of combination may on the reaction kinetics of the various compounds.

In another embodiment of the device, the enzyme or the mediator is coated on the sheet, the co-factor and the other of the mediator or the enzyme are coated onto the working electrode directly, and the sheet is capable of filtering the whole blood such that the active electrode sees a sample which is effectively free of whole blood cells. In this case, the haematocrit dependency of the result is substantially reduced. In this manner, the cell-filtering function of a selected membrane may be combined with the rapid kinetics of having the some or all of the active elements of the reaction (the enzyme, mediator and the co-factor) in the membrane, to produce a highly effective device.

In summary, according to the present invention, a device is constructed by depositing one or more of the reagents required for the quantitation of an analyte as a single or multiple layers on a fine mesh material or membrane; the deposited areas are of dimensions small enough to wet with a very small sample volume. The mesh or membrane can be used in both colorimetric and electrochemical devices.

A characteristic of this invention is that a reagent is applied precisely onto a target area on a woven material such as polyester or nylon or other porous membrane. In use, this provides rapid solubilisation of the reagents in the presence of the sample. The reagent or reagents can be applied in a

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number of different methods that result in the deposition of a known volume at a precise location and in a well-defined foot-print. These include the use of dispensing equipment such as a piston pump, syringe pump or on-demand inkjet printer.

In a further embodiment, a flexible tape containing one or more reagents may be laminated to another flexible tape on which is printed a series of electrodes. Instead of cutting out individual sensors, the laminate (comprising a row or series of sensors) may be used sequentially, e.g. on being dispensed from a suitable dispenser. For this purpose, whether or not as a laminate, a tape of the invention may be provided as a roll, and stored in sealed cassettes which may also contain desiccant. In use, the cassette may be inserted into a automatic dispenser from which the tape is wound out automatically by an indexing mechanism to reveal sequentially the discrete sensors. The action of this instrument is therefore analogous to the action of a film in a camera. In this embodiment, the tape may also contain a red blood cell-lysing reagent such as saponin, in order to reduce the effect of haematocrit and haemoglobin in a whole blood sample. The tape may be further protected from moisture by being covered with a peelable film (e.g. of aluminium) that is automatically peeled off when the tape is dispensed from the cassette. When the sample is applied to the sensor, the amount of analyte of interest in the sample may be determined electrochemically. Such determination can be conducted by known methods.

The following Example illustrates the invention.

Example

A conductive ink material is printed onto a non-conducting polyester sheet material by a screen-printing process. The conductive ink material consists of a mixture of graphite and carbon particles and a polymer binder in an organic solvent. After deposition of the conductive ink, solvents are removed in a forced air oven. A silver/silver chloride reference/counter electrode is printed onto one of each pair of printed carbon electrodes followed by a non-conducting ink layer to define the contact pads and the sensor area.

A mediator such as Meldola Blue, Nile Blue or other suitable dye and the enzyme co-factor nicotinamide adenine dinucleotide (NAD) are deposited onto

the carbon electrode. Alternatively, the NAD is applied separately over the mediator from an aqueous ink.

The enzyme glucose dehydrogenase is deposited as uniform spots on a monofilament polyester mesh tape. This is achieved as follows:

- (a) in a contact mode, where a drop formed at a dispenser tip in close proximity to the mesh is allowed to be transferred to the mesh by touching off the drop onto the mesh surface; or
- (b) in a non-contact mode, where a drop formed by an ink-jet printhead or other orifice above the mesh is dropped onto the mesh from a distance under conditions which do not cause it to penetrate the mesh.

Upon drying, the spots spread to cover an area defined partly by the characteristics of the mesh weave and partly by the application conditions. Typically the areas covered by a 500 nL drop is 1.3 x 1.2 mm. The mesh tape is allowed to dry at room temperature.

The enzyme-modified mesh tape is then laminated onto the modified sheet of devices and secured further by a non-conducting print. Finally, a cover tape is laminated on tope of the mesh. The sheets of devices are disc cut into individual devices. In an alternative device format, the laminated sheets are wound and included in a cassette type unit, allowing a single device to be used by a wind-on mechanism similar to a camera film-winding system.

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CLASSIFICATION OF SUBJECT MATTER PC 7 C12Q1/00 G01 G01N27/30 G01N27/327 G01N35/00 According to international Patent Classification (IPC) or to both national classification and IPC B. FIELDS SZARCHED Minimum documentation searched (classification system followed by classification symbols) C12Q G01N Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched Bectronic data base consulted during the International search (name of data base and, where practical, search terms used) C. DOCUMENTS CONSIDERED TO BE RELEVANT Relevant to cialm No. Citation of document, with indication, where appropriate, of the relevant passages 1-5,10, WO 97 02487 A (BOEHRINGER MANNHEIM CORP) X 23 January 1997 (1997-01-23) 11 page 1, line 33 -page 8, line 28; figure 1: table 1 7-9 Y 1 US 5 169 600 A (ISHIZAKA HIDEO ET AL) X 8 December 1992 (1992-12-08) column 8, line 15-34 7-9 1-5.10. X US 5 779 867 A (SHIEH PAUL) 11 14 July 1998 (1998-07-14) column 4, line 14-21; claims 1-4 abstract -/--Patent family members are listed in annex. Further documents are listed in the continuation of box C. X Special categories of cited documents: "I" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the "A" document defining the general state of the art which is not considered to be of particular relevance Invention "E" earlier document but published on or after the international "X" document of particular relevance; the claimed invention filing date cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "L" document which may throw doubte on priority claim(e) or which is cited to establish the publication date of another "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. citation or other special reason (as specified) "O" document refending to an oral disclosure, use, exhibition or document published prior to the international filing date but "A" document member of the same patent family later than the priority date claimed Date of mailing of the International search report Date of the actual completion of the international search 24/02/2000 11 February 2000 **Authorized officer** Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentiaan 2 NL - 2280 HV Rijawijk Tel. (+31-70) 340-2040, Tx. 31 651 epo ni, Brison, 0 Fax: (+31-70) 340-3016

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CLAIMS

- 1. A test strip comprising a support carrying an active electrode and a counterelectrode, and a layer of material within which a small volume of liquid to be tested can be distributed and provide contact between the electrodes, and wherein an analyte-specific reagent is coated on the material.
- 2. A test strip according to claim 1, wherein the reagent is at least one component of a redox reaction, e.g. one or more of an enzyme, a mediator and/or co-factor for the enzyme.
- 3. A test strip according to claim 2, wherein the at least one component comprises the enzyme.
 - 4. A test strip according to claim 2 or claim 3, wherein the enzyme is glucose oxidase or glucose dehydrogenase.
 - 5. A test strip according to any preceding claim, wherein the material is a monofilament mesh or membrane.
- 6. A flexible tape of a material within which liquid can be distributed and on which are coated discrete areas of at least one component of a redox reaction.
 - 7. A flexible tape according to claim 6, wherein the material is a monofilament mesh or membrane.
 - 8. A container containing a wound tape according to claim 6 or claim 7.
- 9. A container according to claim 8 also comprising automatic dispensing means.
 - 10. A method for testing a liquid for the presence of an analyte, which comprises contacting the liquid with a test strip according to any of claims 1 to 5, and detecting the current.
- 11. A method according to claim 10, wherein the liquid is blood and the analyte is glucose.

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Int. Jonal Application No PCT/GB 99/03764

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	Continuation) DOCUMENT'S CONSIDERED TO BE RELEVANT egory * Citation of document, with indication, where appropriate, of the relevant passages Relevant to claim No					
estegory *	Creation of document, with Endication/where appropriate, or the reserve a personal					
	US 5 798 031 A (CHARLTON STEVEN C ET AL) 25 August 1998 (1998-08-25) abstract	1-5,10, 11				
	column 5, line 22-25	6-8				
	US 5 628 890 A (CARTER NIGEL F ET AL) 13 May 1997 (1997-05-13) column 3, line 41 -column 4, line 10 abstract	1-5,10, 11				
•	EP 0 230 472 A (MATSUSHITA ELECTRIC IND CO LTD) 5 August 1987 (1987-08-05) page 7, line 14-25	1-5,10, 11				
X	EP 0 593 096 A (MEDISENSE INC) 20 April 1994 (1994-04-20) page 6, line 57 -page 7, line 3; figure 3	6–9				
A	page 2, line 28-50	1				
X	US 4 218 421 A (MACK JOHN C JR ET AL) 19 August 1980 (1980-08-19) column 2, line 43 -column 4, line 53	6-9				
X	US 5 679 311 A (HARTTIG HERBERT ET AL) 21 October 1997 (1997-10-21) abstract; figure 2A	6-8				
A,P	W0 99 13100 A (ABBOTT LAB) 18 March 1999 (1999-03-18) abstract; figure 1	1				
	·					
		·				

information on patent family members

Int. Jonel Application No PCT/GB 99/03764

Patent document cited in search rep		Publication date		Patent family member(s)	Publication date
WO 9702487	A	23-01-1997	US	5762770 A	09-06-199
	••	20 02 2007	ĂŬ	712527 B	
			AÜ	6345196 A	
			CA	2224308 A	
			EP	0874984 A	
					
US 5169600	A	08-12-1992	JP	1020454 A	
			JP	2119175 C	
			JP	8020453 B	
			JP	1020455 A	
			JP	2119176 C	06-12-199
			JP	8020454 B	
			JP JP	1080865 A	
			DE	1080866 A 3853700 D	
			DE		
				3853700 T 0299519 A	
			EP		
			US	5122343 A	16-06-199
US 5779867	Α	14-07-1998	US	5522977 A	04-06-199
			US	5645710 A	08-07-199
US 5798031	Α	25-08-1998	AU	6482198 A	12-11-199
			CA	2236132 A	
			ΕP	0878708 A	
			JP	10318971 A	
			NZ	329793 A	
US 5628890	A	13-05-1997	CA	2159553 A	30-03-199
			JP	9222411 A	26-08-199
EP 0230472	A	05-08-1987	JP	2624236 B	25-06-199
			JP	62232554 A	13-10-198
			JP	6048256 B	22-06-199
			JP	61294351 A	
			JP	1915067 C	23-03-199
			JP	6040088 B	25-05-199
			JP	62108145 A	19-05-198
			JP	1949170 C	
			JP	6076984 B	28-09-199
			JP	62108146 A	19-05-198
			JP	1915084 C	23-03-199
			JP	6040089 B	25-05-199
			JP	62137559 A	20-06-198
			DE	3687646 A	11-03-199
			WO	8607632 A	31-12-198
			US	4897173 A	30-01-199
			US	5185256 A	09-02-199
EP 0593096	Α	20-04-1994	AU	622196 B	02-04-199
			AU	3822089 A	01-02-199
			CA	1313397 A	02-02-199
			EP	0352138 A	24-01-199
			JP	2112752 A	25-04-199
			US	5126034 A	30-06-199
US 4218421	A	19-08-1980	NONE		

Form PCT/ISA/210 (patent terrilly annex) (July 1992)

information on patent family members

Int Sonal Application No PCT/GB 99/03764

Patent document cited in search report		Publication date	Patent family member(s)	Publication date
US 5679311	A	21-10-1997	DE 4326339 A EP 0637749 A JP 2610109 B JP 7077528 A US 5609823 A	09-02-1995 08-02-1995 14-05-1997 20-03-1995 11-03-1997
WO 9913100	Α	18-03-1999	AU 9129798 A	29-03-1999

Form PCT/ISA/210 (patent femily ennex) (Ady 1992)

